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Speckle-Tracking Echocardiographic Measures of Right Ventricular Function Correlate with Improvement in Exercise Function after Percutaneous Pulmonary Valve Implantation

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Abstract

Background—Speckle-tracking echocardiographic (STE) measures of right ventricular (RV) function appear to improve after transcatheter pulmonary valve (TPV) implantation. Measures of exercise function, such as ventilatory efficiency (the $V_E/V_{CO_2}$ slope), have been shown to be prognostic of mortality in patients that may require TPV. Our objective was to evaluate the correlation between STE measures of RV function and changes in $V_E/V_{CO_2}$ after TPV placement.

Methods—STE and cardiopulmonary exercise testing were performed at baseline and 6 months after TPV placement in 24 patients from 4 centers. Conventional echocardiographic measures of RV function were also assessed. Echocardiograms and exercise stress tests were interpreted by single blinded observers at separate Core laboratories.

Results—All patients demonstrated relief of pulmonary regurgitation and stenosis after TPV implantation. Improvements in RV longitudinal strain ($-16.9\pm3.5\%$ vs. $-19.7\pm4.3\%$, $p<0.01$) and strain rate ($-0.9\pm0.4\text{s}^{-1}$ vs. $-1.2\pm0.4\text{s}^{-1}$, $p<0.01$) were noted. The $V_E/V_{CO_2}$ slope improved...
(32.4±5.7 vs. 31.5±8.8, p=0.03). No other significant echo or exercise changes were found. Upon multivariable regression, the change in VE/VCO₂ was independently associated with change in RV longitudinal early diastolic strain rate (p<0.001) and tricuspid A velocity (p<0.001). Pre-intervention RV longitudinal strain was found to be a predictor of change in VE/VCO₂ after TPVI (r = −0.60, p<0.001).

**Conclusion**—STE measures of RV function appear to hold the potential for being used as predictors of improved outcomes in patients requiring TPV implantation. Future studies should directly assess the prognostic significance of STE measures of RV function in this population.

**Keywords**

speckle-tracking echocardiography; transcatheter pulmonary valve implantation; congenital heart disease

**Introduction**

Patients with congenital heart disease requiring right ventricular (RV) to pulmonary artery (PA) conduits frequently develop free pulmonary regurgitation, severely dilated RVs, and decreased ventricular function over time.¹ Measures of ventilatory efficiency derived from exercise testing, such as the VE/VCO₂ slope, have been shown to be prognostic of mortality in these patients and are improved after pulmonary valve replacement secondary to improvement in effective stroke volume.²⁻⁷

The relationship between echocardiographic measures of ventricular function and these exercise derived surrogates of outcome are unknown. These patients show little improvement in ventricular function when assessed by traditional echocardiographic markers.⁵ Speckle-tracking echocardiography (STE) measures of ventricular function have been shown to be more sensitive than conventional measures in many disease processes, including in those patients undergoing transcatheter pulmonary valve implantation (TPVI).⁹⁻¹² However, the relationship between STE measures of RV function before and after TPVI and exercise measures are unknown in this population. The objective of this study was to determine the usefulness of assessing RV STE measures of function by assessing their relationship with changes in cardiopulmonary exercise function both before and after TPVI. We hypothesized that RV STE measures of cardiac function would correlate with changes seen in exercise function after TPVI.

**Methods**

This was a retrospective, secondary analysis of data collected during The COgenital Multicenter trial of Pulmonic vAlve regurgitation Studying the SAPIEN interventIONal transcatheter heart valve (COMPASSION) trial. COMPASSION is a prospective, non-randomized, multi-center study to assess the safety and efficacy of the SAPIEN transcatheter heart valve for the treatment of dysfunctional RV-PA conduits. Early phase 1 results have shown good feasibility, effectiveness, and safety.¹³ Patients included in COMPASSION were enrolled prospectively from 4 participating centers. Inclusion criteria included: (1) Weight equal to or exceeding 35 kilograms. (2) In situ conduit size between 16 mm and 24
mm in diameter. (3) Moderate or severe pulmonary regurgitation defined as 3+ pulmonary regurgitation by echocardiogram and/or RV-PA conduit obstruction with a mean gradient of >35 mmHg. (4) Peak VO$_2$ or V$_E$/V$_CO_2$ less than 70% predicted. Informed consent was obtained from all potential subjects and/or their legal guardians. The Institutional Review Board at each participating institution approved the trial.

**Procedure**

The protocol for valve implantation has been reported previously and is summarized here for convenience. Procedures were performed under general anesthesia with biplane fluoroscopic guidance. The minimum diameter of the conduit was assessed by angiography. Risk for coronary compression was assessed with aortic root angiography or selective coronary angiography with simultaneous inflation of a noncompliant balloon in the conduit. Prestenting of the conduit with a bare metal stent was performed. A 23 mm or 26 mm SAPIEN transcatheter heart valve was then implanted over a stiff guidewire and expanded via balloon inflation.

**Echocardiographic protocol**

Analysis of echocardiograms submitted to the COMPASSION core laboratory was performed. Echocardiograms were acquired by experienced sonographers at each center following a protocol which included a complete set of standardized views to evaluate ventricular function. The image acquisition protocol was developed by the echocardiography core laboratory. On-site or web-based training to the local SAPIEN TPV implantation sites was provided. Echocardiograms utilized for this analysis were performed at baseline prior to TPV implantation, prior to discharge after TPV implantation, 30-day follow-up, and 6-month follow-up. All studies were performed under baseline physiologic conditions, not under the influence of anesthesia. Measures were recorded at end expiration with quiet respiration. Pre-TPV echos were performed ≤1 week prior to TPV implantation.

Echocardiograms were in DICOM format. All measurements were made off line by a single reviewer and averaged over 3 beats. Pulmonary regurgitation was graded from 0 to 4 based on jet width:annulus ratio and flow reversal in the branch pulmonary arteries as follows: 0 = no regurgitation, 1 = jet width:annulus < 0.25, 2 = jet width:annulus between 0.25 and 0.5, 3 = jet width:annulus between 0.5 and 0.7, 4 = jet width:annulus > 0.7 with flow reversal in the branch pulmonary arteries. Tricuspid valve regurgitant orifice area was calculated from the apical four chamber and parasternal short axis windows.

**Two-dimensional, spectral, and tissue Doppler measures of myocardial function**

From a standard apical four-chamber window, RV fractional area change (FAC) was defined as ((end-diastolic area – end-systolic area)/end-diastolic area) x 100. Tricuspid annular plane systolic excursion (TAPSE) was obtained, and indexed TAPSE was calculated as ((RV end-diastolic length – RV end-systolic length)/RV end-diastolic length). Pulsed tissue Doppler imaging (TDI) S’ velocities at the tricuspid valve annulus and interventricular septum were obtained from the apical four-chamber view.

To evaluate diastolic function, Doppler velocities of transtricuspid flow (E and A) were obtained from an apical four-chamber window. Tissue Doppler velocities of the tricuspid...
annulus and interventricular septum (E’ and A’) were obtained. Derived ratios (E:A, E:E’) were calculated.

### Speckle-tracking echocardiography measures of myocardial function

Speckle-tracking was performed as a secondary analysis of echocardiograms submitted to COMPASSION echocardiography core laboratory. A single, blinded observer performed offline analysis of DICOM images using vendor-independent software (2D Cardiac Performance Analysis v. 3.0, TomTec Imaging Systems, Inc, Munich, Germany). Myocardial motion was tracked through the cardiac cycle, calculating myocardial deformation from echogenic speckles in the B-mode image. Endocardium and epicardium were manually traced in the RV from the lateral tricuspid annulus to the septal component of the tricuspid annulus (Figure 1). The septum was included secondary to its importance to global RV function. End-systole was defined as end ejection of the pulmonic valve for the RV and of the aortic valve for the LV using spectral Doppler. Speckle-tracking measures of deformation from the apical 4-chamber view included peak longitudinal strain, strain rate, and early diastolic strain rate. Left ventricular measures of deformation from the apical 4-chamber view were also assessed. Global deformation measurements were calculated as an average of 6 segments. Tracking was visually assessed, and deformation curves were not accepted if greater than one segment demonstrated inadequate tracking. It should be noted that longitudinal strain is by convention expressed using negative numbers. When describing relative differences, the absolute value of the strain amplitude (ignoring the minus sign) is referenced. For example, a strain of −23% represents better function than a strain of −13%.

### Exercise protocol

All patients underwent a symptom limited cardiopulmonary exercise test with progressive protocols using either a bicycle ergometer or treadmill depending on the available equipment in the individual centers. Patients had a rest period to capture baseline, then a warm up period without load, followed by an increase of load depending on the expected individual physical capacity as estimated by the investigator. The end of the exercise test was marked by symptom limitation and was followed by a recovery period. All exercise tests were analyzed by a blinded observer in a separate COMPASSION cardiopulmonary testing Core laboratory.

The exercise test used breath-by-breath gas exchange analysis via a metabolic cart. The primary exercise measure of interest was ventilatory efficiency as analyzed by the $V_{E}/V_{CO_2}$ slope. Peak oxygen uptake ($VO_2$) was defined as the highest mean uptake during exercise. Anaerobic threshold (AT) was determined by use of the modified V-slope method. Peak O$_2$ pulse was defined as peak VO$_2$ divided by peak heart rate.

### Statistical Analysis

Paired t-tests were used to assess for changes in exercise test variables between baseline and 6 months. For echocardiograms, to determine the trend from time 0 to time 3, repeated measures ANOVA with a Greenhouse-Geisser correction was conducted on all individuals with measurements for each of the four time points. Post hoc comparisons using the Bonferroni correction were then performed in those variables which showed a statistically
significant repeated measure ANOVA. Missing data was not imputed as numbers were sufficient to conduct appropriate analyses. Pearson's correlation and multiple variable stepwise linear regression were used to assess for a linear relationship between echocardiographic variables and exercise function. Independent variables assessed with stepwise regression techniques included baseline and % change in: RV size (end-diastolic and systolic area), conduit peak and mean gradients, and all measures of RV and LV systolic function as described above. Age and sex were also included in the analysis. Results of multivariable analysis are reported as partial correlations - its purpose is to quantify the association between two variables while eliminating the variance from other variables in the model. A receiver operating characteristic (ROC) curve was developed to assess the sensitivity and specificity of optimal cutoff values for the pre-operative echocardiographic variable that best predicts an improvement in exercise function. Intra- and inter-observer variability was assessed by absolute percent error of the mean (the difference between the two measurements was divided by the mean of those two measurements) and by intraclass correlation coefficient (ICC) using a random effects model measuring absolute agreement. An ICC of ≥0.75 was deemed acceptable intra- or inter-observer variability. A p-value < 0.05 was considered significant. Statistics were analyzed using SPSS v. 22 (IBM, New York, NY, USA).

Results

The first 33 patients from 4 centers who had successful SAPIEN TPV implantation in the COMPASSION trial were eligible. A total of 132 echocardiograms were performed. Of these, 17 echocardiograms were excluded for inability to perform STE due to inadequate RV free wall and/or apical segment capture in the echocardiographic window, or, for inadequate apical four-chamber windows. These 17 echocardiograms came from a total of 9 patients. Therefore, 24 patients had echocardiograms suitable for speckle-tracking analysis (≤2 segments were excluded from the RV analysis) at each of the four time points so that a comprehensive analysis of changes in ventricular function after TPVI could be performed. Demographic data from these patients are presented in Table 1. After TPV implantation no patient had greater than mild stenosis or regurgitation.

Changes after TPV implantation

Peak and mean gradients through the conduit, pulmonary regurgitation grade, RV enddiastolic and systolic areas, and tricuspid regurgitation velocity decreased between baseline and six months (Table 2). No significant changes were detected in the conventional measures of RV systolic or diastolic function at 6 month follow-up with the exception of an increase in tricuspid inflow Doppler A velocity (Table 3). Statistically significant improvements in RV longitudinal strain and strain rate were noted while changes in RV early diastolic strain rate trended toward significance (Table 4). The $V_e/V_{CO_2}$ slope and $O_2$ pulse improved between baseline and 6 months; in contrast, there were no statistically significant changes in peak $VO_2$, $VO_2$ at AT, or respiratory exchange ratio at AT (Table 5).
Changes in echocardiographic measures vs. changes in exercise measures

Changes in conventional echocardiographic measures of RV function did not correlate with changes in measures of exercise function. Further, changes in echocardiographic measures of RV size, conduit stenosis, conduit insufficiency, and tricuspid regurgitant jet gradient did not correlate with changes in measures of exercise function. The change in $V_{E}/V_{CO2}$ correlated with the change in RV longitudinal strain ($r = 0.54$, $p = 0.02$) (Figure 2) and early diastolic strain rate ($r = -0.59$, $p = 0.01$) (Figure 3). No other correlations were found between changes in STE measures of function and exercise measures of function. No correlations were found between changes in LV measures of deformation and changes in exercise function variables. Upon multiple variable regression, only % change in RV early diastolic strain rate and tricuspid valve inflow Doppler A velocity demonstrated a statistically significant relationship with % change in $V_{E}/V_{CO2}$ (Table 6). No variables demonstrated collinearity (variance inflation factors for all variables < 5).

Pre-intervention echocardiographic measures vs. changes in exercise measures

Pre-TPVI echocardiographic measures of RV size, conduit insufficiency, and tricuspid regurgitant jet gradient did not correlate with changes in measures of exercise function. The change in $V_{E}/V_{CO2}$ correlated with the pre-TPVI RV longitudinal strain ($r = -0.60$, $p < 0.01$) and conduit mean gradient ($r = -0.48$, $p = 0.05$). No other correlations were found between changes in STE measures of function and exercise measures of function. Pre-TPVI mitral Doppler E:A ($r = -0.71$, $p < 0.01$), tricuspid E:E' ($r = -0.56$, $p = 0.01$), and tricuspid septal S velocity ($r = 0.57$, $p < 0.01$) correlated with change in $O_2$ pulse. No correlation between baseline LV measures of deformation and changes in exercise function variables were found. Upon multiple variable regression, only pre-TPVI RV longitudinal strain demonstrated a statistically significant relationship with % change in $V_{E}/V_{CO2}$ (Table 7). No variables demonstrated collinearity (variance inflation factors for all variables < 5). ROC curve for pre-TPVI RV longitudinal strain to predict an improvement in $V_{E}/V_{CO2}$ greater than 5% of baseline showed a c-statistic (area under the curve) of 0.75 (Figure 4).

STE observer variability

Intra- and inter-observer variability of STE measures of deformation were performed in 25% ($n = 24$) of the studies. Results are presented in Table 8. All observer measurement variability was deemed acceptable.

Discussion

Speckle-tracking measures of deformation have been shown to be more sensitive than conventional measures in detecting changes in myocardial function in multiple disease processes.9-11 We have reported similar findings in the current cohort.12 However, the clinical utility of detecting these changes by STE is unknown in this population. A number of groups have shown that measures of exercise function, specifically peak VO$_2$ and $V_{E}/V_{CO2}$, predict risk of morbidity and mortality in patients with repaired Tetralogy of Fallot and other forms of congenital heart disease.4-7, 17 Therefore, to assess STE measures’ potential to be used as surrogates for outcome, we assessed the correlation between STE measures of deformation and changes in measures of exercise function after TPVI. We
found that changes in STE early diastolic strain rate correlated with changes in $\frac{V_E}{V_{CO_2}}$. In addition, pre-TPVI RV longitudinal strain correlated with $\frac{V_E}{V_{CO_2}}$ response to TPVI. These findings support the potential clinical usefulness of assessing RV function using STE prior to and after TPVI.

Patients with dysfunctional RV to PA conduits exhibit decreased VO$_2$, $\frac{V_E}{V_{CO_2}}$, and O$_2$ pulse upon exercise testing and are often symptomatic.$^{18}$ Despite the fact that patient symptoms improved significantly in this cohort as previously reported (85% of patients were NYHA Class II-IV pre-TPVI vs. 15% post-TPVI),$^{13}$ patients in the current study showed no change in peak VO$_2$, VO$_2$ at AT, or RER after TPVI. This is in line with previous studies that showed similar findings.$^2$-$^3$, $^6$, $^{19}$-$^{21}$ Many studies use VO$_2$ as the primary outcome of interest after pulmonary valve replacement. However, using VO$_2$ as the primary measure of cardiovascular health in this population may be misleading. This is because VO$_2$ is influenced by both respiratory and cardiovascular health, with no way to differentiate between the two. In fact, the majority of patients with chronic pulmonary regurgitation have a primary respiratory limitation to peak VO$_2$, rather than a cardiovascular limitation.$^{22}$ Pulmonary valve replacement does not improve this respiratory limitation, therefore VO$_2$ is unchanged.

In contrast, $\frac{V_E}{V_{CO_2}}$ accounts for both respiratory ($V_E$) and cardiovascular ($V_{CO_2}$) influences to exercise function. It will detect changes in the cardiovascular contribution to exercise function even if the respiratory component is unchanged. Improvement in $\frac{V_E}{V_{CO_2}}$ has been reported after both surgical and transcatheter pulmonary valve replacement in patients with predominantly pulmonary regurgitation or mixed disease, similar to the findings in the current study.$^2$, $^3$ $\frac{V_E}{V_{CO_2}}$ is a measure of ventilatory efficiency and thought to improve after TPVI secondary to improved effective RV stroke volume and/or cardiac output. This is supported by the fact that a surrogate of LV stroke volume, the peak O$_2$ pulse, improved in our study, and others,$^{19}$, $^{23}$ after TPVI suggesting improved LV preload.

Percent change in RV longitudinal strain and early diastolic strain rate correlated with percent change in $\frac{V_E}{V_{CO_2}}$. Multivariable analysis revealed that only diastolic measures demonstrated a relationship with change in $\frac{V_E}{V_{CO_2}}$. Diastolic function has been suggested to be associated with exercise capacity in this patient group by others.$^{21}$ These findings suggest that change in RV diastolic function may be an important determinant of the change in cardiac output that drives resultant $\frac{V_E}{V_{CO_2}}$ after TPVI. Therefore, these measurements of RV diastolic function may be clinically useful to follow before and after TPVI.

There were no significant correlations between traditional measures of RV function and exercise function in the current study. Menon et al. reported similar findings in a group with pulmonary regurgitation.$^{24}$ Hasan et al. showed that there are correlations between RV STE longitudinal strain and peak VO$_2$ both before and after TPVI in a group with obstructed conduits.$^{23}$ These studies support the additive value of STE over conventional echocardiography in this population.

While STE measures of deformation are more load-resistant than conventional measures of function, they are not load independent. The association we found between STE measures

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and \( \text{VE/VCO}_2 \) may be confounded by the loading changes after TPVI. Unfortunately, as reported previously by Kenny et al.,\textsuperscript{13} change in RV volumes and pulmonary regurgitant fraction were available in less than half of patients (n = 13) in the initial cohort (n = 33) due to artifact from the stainless steel stent. In patients with MRI data, right ventricular volumes (130 ± 63 ml/m\(^2\) to 87 ± 20 ml/m\(^2\), p = 0.02) and pulmonary regurgitant fraction (29 ± 18% to 3.5±5.4%, p < 0.01) improved following TPVI. To attempt to determine whether changes in RV STE measures of deformation were indeed representative of changes in RV performance, we attempted to control for changes in RV size by including echocardiographic end-diastolic area and end-systolic area in the multivariable model; they were not predictive of changes in exercise parameters. In addition, RV STE measures of deformation did not change with acute changes in loading conditions, i.e. no change was seen between baseline and discharge after TPVI. There was also no change at one month follow-up when RV size reached its nadir. RV STE measures of deformation did not change with acute changes in loading conditions, i.e. no change was seen between baseline and discharge after TPVI. In a cohort identical to the one in this study, a baseline RV longitudinal strain greater than −18% would have an 82% sensitivity and 71% specificity in detecting a positive response to TPVI as defined by a > 5% improvement in \( \text{VE/VCO}_2 \). However, this is an ideal scenario, the diagnostic performance of RV strain in predicting improvement in \( \text{VE/VCO}_2 \) needs to be independently assessed in a separate cohort. Sabate Rotes et al. found RV longitudinal strain as the only independent predictor for an improvement in NYHA heart failure class after surgical pulmonary valve replacement.\textsuperscript{25} Traditional echocardiographic surrogates for MRI EF, such as RV FAC, did not show a similar relationship. It appears RV longitudinal strain holds potential as a pre-intervention predictor of outcomes and deserves further study. It may be especially useful in patients with borderline RV volumes and normal EF who have pulmonary regurgitation or mixed disease.

**Limitations**

There were limitations to this study. The sample was small and heterogeneous in age, diagnosis, and type of conduit dysfunction. The primary diagnosis in five patients were not available as they did not have Tetralogy of Fallot or the Ross procedure. This may have implications as regional abnormalities in RV function can be expected if reconstruction of the RV outflow tract was performed, leaving regional of measures of function, such as TAPSE, inaccurate as a measure of global RV function. This was a secondary analysis of prospectively collected data. Thus, the echocardiographic protocol was not designed with STE in mind. This resulted in nine patients being excluded from this analysis. Most patients...
were excluded for RV free wall and apical segments being inadequately captured in the
echocardiographic window. Future protocols using STE post TPV implantation should stress
the importance of optimal image acquisition including all RV segments. The percentage of
success in obtaining adequate images for speckle-tracking analysis of the RV should then be
assessed. In addition, echocardiograms were compressed and stored at 30 frames per second
when read by the core lab. While strain measures are accurate at this frame rate, strain rate
can be underestimated, which may confound our results. We were only able to measure
longitudinal strain. Circumferential strain has been shown to be important in pressure-loaded
RVs, but could not be measured due to limitations in the acquisition protocol.

It is known that patients with conduit stenosis display more improved exercise function after
valve replacement than patients with pulmonary regurgitation. However, many of the
patients in this cohort had mixed disease, which makes it difficult to compare our exercise
results with previous studies as those with mixed disease may display traits of both those
with stenosis only and regurgitation only. We measured RV size using RV areas from the
apical four chamber windows. While echocardiography is certainly not the gold standard
method to measure RV size, it has shown good correlation to MRI values. This may
become more important as the use of TPVI increases, as stainless steel stent implantation
can decrease the success rate of obtaining RV volumes by MRI. Many known factors that
influence outcomes in these patients were not accounted for secondary to unavailability of
data or due to the small, heterogeneous nature of the sample, including age at first operation,
age since last operative repair, type of conduit dysfunction, type of congenital heart disease,
RV volumes derived from MRI, degree of impairment in ventriculo-ventricular interactions,
evidence of post-systolic shortening, forward flow in the pulmonary artery during atrial
systole, other echocardiographic surrogates of right atrial pressure, QRS duration,
arrhythmias, and evidence of mechanical dyssynchrony. Larger studies will be
needed to determine the usefulness of RV STE measures of deformation in the peri-TPVI
period when these other factors are accounted for. The lack of an age-matched control group
does not allow us to have a frame of reference when assessing the effect TPVI on RV
function in relation to healthy individuals.

Conclusion

Improvements are seen in exercise function, as measured by the $V_E/V_{CO_2}$ ratio, six months
post-TPVI in patients with conduits that are purely regurgitant or display mixed disease.
Improvements in RV diastolic function may contribute to the changes in exercise
performance seen after TPVI. Abnormal pre-intervention RV longitudinal strain may be a
predictor for improved exercise function after TPVI. STE measures of RV function appear
to hold the potential for being used as predictors of improved clinical outcomes in patients
requiring TPV implantation. Future studies should directly assess the prognostic significance
of STE measures of RV function in this population.

Acknowledgements

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**Abbreviations**

AT  anaerobic threshold  
FAC  fractional area change  
PA  pulmonary artery  
STE  speckle-tracking echocardiography  
TAPSE  tricuspid annular plane systolic excursion  
TDI  tissue Doppler imaging  
TPVI  transcatheater pulmonary valve implantation  

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Highlights

- Improvements are seen in RV STE measures of deformation and $V_E/V_{CO_2}$ six months post-TPVI in patients with conduits that are purely regurgitant or display mixed disease.
- Changes in STE measures of RV diastolic function correlate with changes seen in $V_E/V_{CO_2}$ after TPVI.
- Patients with decreased pre-intervention RV longitudinal strain have a higher likelihood to display improved $V_E/V_{CO_2}$ after TPVI than those without.
- STE measures of RV function appear to hold the potential for being used as predictors of improved outcomes in patients requiring TPV implantation.
Figure 1. STE of the RV
Two-dimensional speckle tracking echocardiogram of RV longitudinal strain in a patient with Tetralogy of Fallot with mixed conduit stenosis and insufficiency. Endocardial and epicardial traces are shown.
Figure 2. Percent change in RV LS vs. $V_E/V_{CO_2}$
Scatter plot with linear regression line showing the relationship between % change in $V_E/V_{CO_2}$ and RV longitudinal strain.
Figure 3. Percent change in RV EDSR vs. $V_E/V_{CO_2}$
Scatter plot with linear regression line showing the relationship between % change in $V_E/V_{CO_2}$ and RV longitudinal strain.
Figure 4. ROC curve
Receiver operating characteristic analysis to depict pre-intervention RV longitudinal strain's ability to predict a > 5% increase in post-intervention $V_E/V_{CO_2}$, area under the curve = 0.75.
### Table I

**Patient Demographics**

<p>| | |</p>
<table>
<thead>
<tr>
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<tbody>
<tr>
<td>Age, yrs</td>
<td>32.3 ± 17.0</td>
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<tr>
<td>Weight, kg</td>
<td>73.5 ± 24.1</td>
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<td>Male/female</td>
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<td>Ross procedure</td>
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<tr>
<td>Other</td>
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<tr>
<td>Mixed</td>
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<tr>
<td>Pulmonary stenosis grade</td>
<td></td>
</tr>
<tr>
<td>None (&lt;16 mmHg)</td>
<td>4</td>
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<tr>
<td>Mild (16-30 mmHg)</td>
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</tr>
<tr>
<td>Moderate (31–45 mmHg)</td>
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</tr>
<tr>
<td>Severe (&gt;45 mmHg)</td>
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<tr>
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</tr>
<tr>
<td>Trivial</td>
<td>0</td>
</tr>
<tr>
<td>Mild</td>
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</tr>
<tr>
<td>Moderate</td>
<td>1</td>
</tr>
<tr>
<td>Severe</td>
<td>22</td>
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Pulmonary stenosis was graded based on net peak gradient. Pulmonary regurgitation was graded based on jet width:annulus ratio and flow reversal in the branch pulmonary arteries as follows: None = no regurgitation, trivial = jet width:annulus < 0.25, mild = jet width:annulus between 0.25 and 0.5, moderate = jet width:annulus between 0.5 and 0.7, severe = jet width:annulus > 0.7 with flow reversal in the branch pulmonary arteries.
Table 2
Pulmonary and tricuspid valve function and right ventricular size after TPV implantation

<table>
<thead>
<tr>
<th>Measure</th>
<th>Baseline (time 0)</th>
<th>Discharge (time 1)</th>
<th>30-day follow-up (time 2)</th>
<th>6-month follow-up (time 3)</th>
<th>ANOVA (p-value)</th>
<th>Multiple Comparison (p &lt; 0.05)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Conduit stenosis peak gradient (mm Hg)</td>
<td>42.4 ± 5.5</td>
<td>22.1 ± 2.1</td>
<td>22.3 ± 3.1</td>
<td>20.7 ± 2.6</td>
<td>&lt;0.01</td>
<td>Time 0 vs 1, 2, 3</td>
</tr>
<tr>
<td>Conduit stenosis mean gradient (mm Hg)</td>
<td>24.1 ± 3.2</td>
<td>13.2 ± 1.3</td>
<td>13.1 ± 1.8</td>
<td>12.3 ± 1.7</td>
<td>&lt;0.01</td>
<td>Time 0 vs 1, 2, 3</td>
</tr>
<tr>
<td>RV end-diastolic area (cm²)</td>
<td>41.4 ± 1.9</td>
<td>42.3 ± 2.3</td>
<td>37.6 ± 2.0</td>
<td>37.1 ± 1.6</td>
<td>&lt;0.01</td>
<td>Time 0 vs 2, 3 Time 1 vs 2, 3</td>
</tr>
<tr>
<td>RV end-systolic area (cm²)</td>
<td>29.3 ± 1.3</td>
<td>29.7 ± 2.0</td>
<td>26.1 ± 1.6</td>
<td>25.4 ± 1.0</td>
<td>&lt;0.01</td>
<td>Time 0 vs 3 Time 1 vs 2, 3</td>
</tr>
<tr>
<td>TR peak gradient (mm Hg)</td>
<td>56.2 ± 5.1</td>
<td>47.1 ± 3.2</td>
<td>40.2 ± 2.6</td>
<td>40.9 ± 2.6</td>
<td>&lt;0.01</td>
<td>Time 0 vs 2, 3 Time 1 vs 2</td>
</tr>
<tr>
<td>Indexed TR jet area (cm²/m²)</td>
<td>0.18 ± 0.20</td>
<td>0.11 ± 0.12</td>
<td>0.11 ± 0.17</td>
<td>0.10 ± 0.09</td>
<td>&lt;0.01</td>
<td>Time 0 vs 1, 2, 3</td>
</tr>
<tr>
<td>Tricuspid Valve Annulus Z-score</td>
<td>1.36 ± 0.94</td>
<td>1.41 ± 0.99</td>
<td>1.49 ± 1.00</td>
<td>1.64 ± 0.80</td>
<td>0.89</td>
<td>none</td>
</tr>
</tbody>
</table>

Values are mean ± SD, p-values, or time-points where differences in measures were statistically significant by multiple comparison test. RV = right ventricular, TR = tricuspid regurgitation.
Table 3
Changes in conventional measures of cardiac function after TPV implantation

<table>
<thead>
<tr>
<th>Measure</th>
<th>Baseline (time 0)</th>
<th>Discharge (time 1)</th>
<th>30-day Follow-up (time 2)</th>
<th>6-month Follow-up (time 3)</th>
<th>ANOVA (p-value)</th>
<th>Multiple Comparison (p &lt; 0.05)</th>
</tr>
</thead>
<tbody>
<tr>
<td>RV FAC (%)</td>
<td>29.0 ± 1.9</td>
<td>30.1 ± 1.7</td>
<td>29.2 ± 2.0</td>
<td>31.4 ± 1.1</td>
<td>0.72</td>
<td>n/a</td>
</tr>
<tr>
<td>TAPSEi (%)</td>
<td>0.14 ± 0.01</td>
<td>0.15 ± 0.01</td>
<td>0.15 ± 0.01</td>
<td>0.16 ± 0.01</td>
<td>0.48</td>
<td>n/a</td>
</tr>
<tr>
<td>TDI: Tricuspid S (cm/sec)</td>
<td>7.7 ± 0.5</td>
<td>9.1 ± 0.4</td>
<td>8.0 ± 0.4</td>
<td>8.2 ± 0.4</td>
<td>&lt;0.01</td>
<td>Time 0 vs 1</td>
</tr>
<tr>
<td>RV Doppler E (cm/sec)</td>
<td>72.6 ± 5.5</td>
<td>77.9 ± 5.1</td>
<td>76.6 ± 5.7</td>
<td>70.3 ± 3.7</td>
<td>0.31</td>
<td>n/a</td>
</tr>
<tr>
<td>RV Doppler A (cm/sec)</td>
<td>44.9 ± 4.0</td>
<td>59.1 ± 5.5</td>
<td>51.1 ± 4.4</td>
<td>49.2 ± 4.9</td>
<td>0.02</td>
<td>n/a</td>
</tr>
<tr>
<td>RV Doppler E:A</td>
<td>1.8 ± 0.2</td>
<td>1.5 ± 0.2</td>
<td>1.6 ± 0.2</td>
<td>1.7 ± 0.2</td>
<td>0.37</td>
<td>n/a</td>
</tr>
<tr>
<td>TDI: Tricuspid e’ (cm/sec)</td>
<td>7.9 ± 2.1</td>
<td>8.9 ± 2.1</td>
<td>7.8 ± 1.7</td>
<td>7.9 ± 1.7</td>
<td>&lt;0.01</td>
<td>Time 0 vs 1</td>
</tr>
<tr>
<td>TDI: Tricuspid E:e’</td>
<td>7.4 ± 0.9</td>
<td>8.4 ± 0.7</td>
<td>9.3 ± 1.2</td>
<td>8.3 ± 0.8</td>
<td>0.29</td>
<td>n/a</td>
</tr>
</tbody>
</table>

Results are reported in mean ± standard deviation. FAC = fractional area change, RV = right ventricle, TAPSEi = indexed tricuspid annular systolic plane excursion, TDI = tissue Doppler imaging.
## Table 4

Changes in STE Measures of Function

<table>
<thead>
<tr>
<th>Measure</th>
<th>Baseline (time 0)</th>
<th>Discharge (time 1)</th>
<th>30-day Follow-up (time 2)</th>
<th>6-month Follow-up (time 3)</th>
<th>ANOVA (p-value)</th>
<th>Multiple Comparison (p &lt; 0.05)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Global RV LS (%)</td>
<td>−16.9 ± 0.7</td>
<td>−17.3 ± 1.0</td>
<td>−17.8 ± 0.6</td>
<td>−19.6 ± 0.9</td>
<td>&lt; 0.01</td>
<td>Time 0 vs 3</td>
</tr>
<tr>
<td>Global RV LSR</td>
<td>−0.87 ± 0.09</td>
<td>−1.03 ± 0.07</td>
<td>−1.03 ± 0.05</td>
<td>−1.16 ± 0.08</td>
<td>0.01</td>
<td>Time 0 vs 3</td>
</tr>
<tr>
<td>Global RV LEDSR (s⁻¹)</td>
<td>1.11 ± 0.10</td>
<td>1.16 ± 0.11</td>
<td>1.12 ± 0.09</td>
<td>1.31 ± 0.10</td>
<td>0.15</td>
<td>n/a</td>
</tr>
<tr>
<td>RV free wall LS (%)</td>
<td>−17.0 ± 3.7</td>
<td>−17.2 ± 6.1</td>
<td>−19.1 ± 4.8</td>
<td>−21.9 ± 6.2</td>
<td>&lt; 0.01</td>
<td>Time 0 vs 3</td>
</tr>
<tr>
<td>RV free wall LSR (s⁻¹)</td>
<td>−0.98 ± 0.33</td>
<td>−1.04 ± 0.39</td>
<td>−1.11 ± 0.30</td>
<td>−1.31 ± 0.68</td>
<td>0.04</td>
<td>Time 0 vs 3, Time 1 vs 3</td>
</tr>
<tr>
<td>RV free wall LEDSR (s⁻¹)</td>
<td>1.10 ± 0.48</td>
<td>1.16 ± 0.56</td>
<td>1.27 ± 0.61</td>
<td>1.43 ± 0.64</td>
<td>0.11</td>
<td>n/a</td>
</tr>
<tr>
<td>Septal LS (%)</td>
<td>−16.0 ± 3.9</td>
<td>−16.5 ± 4.5</td>
<td>−15.9 ± 2.9</td>
<td>−17.8 ± 5.4</td>
<td>0.30</td>
<td>n/a</td>
</tr>
<tr>
<td>Septal LSR (s⁻¹)</td>
<td>−0.91 ± 0.24</td>
<td>−1.01 ± 0.35</td>
<td>−0.93 ± 0.27</td>
<td>−1.05 ± 0.42</td>
<td>0.22</td>
<td>n/a</td>
</tr>
<tr>
<td>Septal LEDSR (s⁻¹)</td>
<td>1.10 ± 0.46</td>
<td>1.08 ± 0.49</td>
<td>0.97 ± 0.34</td>
<td>1.17 ± 0.46</td>
<td>0.29</td>
<td>n/a</td>
</tr>
<tr>
<td>Global LV LS (%)</td>
<td>−16.2 ± 0.8</td>
<td>−18.5 ± 0.8</td>
<td>−18.0 ± 1.1</td>
<td>−18.2 ± 0.9</td>
<td>0.01</td>
<td>Time 0 vs 3</td>
</tr>
<tr>
<td>Global LV LSR (s⁻¹)</td>
<td>−1.13 ± 0.09</td>
<td>−1.18 ± 0.07</td>
<td>−1.11 ± 0.08</td>
<td>−1.06 ± 0.15</td>
<td>0.69</td>
<td>n/a</td>
</tr>
<tr>
<td>Global LV LEDSR (s⁻¹)</td>
<td>1.28 ± 0.08</td>
<td>1.34 ± 0.11</td>
<td>1.30 ± 0.10</td>
<td>1.32 ± 0.09</td>
<td>0.90</td>
<td>n/a</td>
</tr>
</tbody>
</table>

Results are reported in mean ± standard deviation. LEDSR = longitudinal early diastolic strain rate, LS = longitudinal strain, LSR = longitudinal strain rate, LV = left ventricular, RV = right ventricular.
### Table 5

Changes in Exercise Parameters

<table>
<thead>
<tr>
<th>Measure</th>
<th>Baseline</th>
<th>6-month</th>
<th>p-value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Peak VO$_2$ (mL/kg/min)</td>
<td>24.1 ± 10.3</td>
<td>25.5 ± 8.2</td>
<td>0.18</td>
</tr>
<tr>
<td>VO$_2$ at AT (mL/kg/min)</td>
<td>14.1 ± 5.2</td>
<td>15.0 ± 5.1</td>
<td>0.53</td>
</tr>
<tr>
<td>RER at AT</td>
<td>0.89 ± 0.09</td>
<td>0.91 ± 0.10</td>
<td>0.94</td>
</tr>
<tr>
<td>V$\text{CO}_2$/V$\text{O}_2$ at AT</td>
<td>32.4 ± 5.7</td>
<td>29.5 ± 8.8</td>
<td>0.02</td>
</tr>
<tr>
<td>$\text{O}_2$ Pulse (mL/beat)</td>
<td>10.9 ± 3.4</td>
<td>12.1 ± 3.8</td>
<td>0.01</td>
</tr>
</tbody>
</table>

Results are reported in mean ± standard deviation. AT = anaerobic threshold, RER = respiratory exchange ratio.
Table 6

Results of Stepwise Multivariable Linear Regression Analysis Assessing Changes in Echocardiographic Measures of Pulmonary Valve Function, RV Size, and RV Function to % Change in $V_E/V_{CO_2}$

<table>
<thead>
<tr>
<th>Model</th>
<th>Variable</th>
<th>B</th>
<th>SE</th>
<th>$\beta$</th>
<th>t</th>
<th>Partial R</th>
<th>p</th>
<th>F</th>
<th>R</th>
<th>$R^2$</th>
</tr>
</thead>
<tbody>
<tr>
<td>1</td>
<td>Constant</td>
<td>7.33</td>
<td>2.44</td>
<td>3.00</td>
<td>6.35</td>
<td>0.03</td>
<td>0.33</td>
<td>&lt;0.01</td>
<td>10.63</td>
<td>0.64</td>
</tr>
<tr>
<td></td>
<td>% change RV EDSR</td>
<td>-0.13</td>
<td>0.05</td>
<td>-0.57</td>
<td>-2.52</td>
<td>0.01</td>
<td>0.57</td>
<td>&lt;0.01</td>
<td>6.80</td>
<td>0.33</td>
</tr>
<tr>
<td>2</td>
<td>Constant</td>
<td>8.70</td>
<td>1.91</td>
<td>4.55</td>
<td>&lt;0.01</td>
<td></td>
<td></td>
<td>&lt;0.01</td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>% change RV EDSR</td>
<td>-0.14</td>
<td>0.04</td>
<td>-0.61</td>
<td>-3.53</td>
<td>0.71</td>
<td>&lt;0.01</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>% change TV A velocity</td>
<td>0.12</td>
<td>0.04</td>
<td>0.56</td>
<td>3.22</td>
<td>0.68</td>
<td>&lt;0.01</td>
<td></td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

Results of stepwise multiple variable linear regression analysis above. No other measures of changes in pulmonary valve function, RV size, and RV function met criteria for entrance into the model. A p value of < 0.05 was considered significant. EDSR = early diastolic strain rate, RV = right ventricular, TV = tricuspid valve.
Table 7
Results of Stepwise Multivariable Linear Regression Analysis Assessing Pre-intervention Echocardiographic Measures of Pulmonary Valve Function, RV Size, and RV Function to % Change in $V_E/V_{CO_2}$ Post-intervention

<table>
<thead>
<tr>
<th>Model</th>
<th>Variable</th>
<th>B</th>
<th>SE</th>
<th>$\beta$</th>
<th>t</th>
<th>P</th>
<th>F</th>
<th>R</th>
<th>$R^2$</th>
</tr>
</thead>
<tbody>
<tr>
<td>1</td>
<td>Constant</td>
<td>35.84</td>
<td>9.33</td>
<td>3.84</td>
<td>&lt;0.01</td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td></td>
<td>RV LS</td>
<td>1.61</td>
<td>0.57</td>
<td>0.59</td>
<td>2.84</td>
<td>0.01</td>
<td></td>
<td></td>
<td></td>
</tr>
</tbody>
</table>

Results of stepwise multiple variable linear regression analysis above. All other measures of pre-intervention pulmonary valve function, RV size, and RV function did not meet criteria for entrance into the model. A $p$ value of < 0.05 was considered significant. EDSR = early diastolic strain rate, RV = right ventricular, TV = tricuspid valve.
### Table 8

Intraobserver and interobserver variability of speckle-tracking measures of ventricular function

<table>
<thead>
<tr>
<th></th>
<th>Intraobserver % Error of the Mean (%)</th>
<th>Intraobserver ICC (r value)</th>
<th>Interobserver % Error of the Mean (%)</th>
<th>Interobserver ICC (r value)</th>
</tr>
</thead>
<tbody>
<tr>
<td>RV LS</td>
<td>0.1 (−5.2 – 2.9)</td>
<td>0.93</td>
<td>3.1 (−10.5 – 3.6)</td>
<td>0.75</td>
</tr>
<tr>
<td>RV LSR</td>
<td>0.4 (−9.1 – 10.3)</td>
<td>0.88</td>
<td>−3.3 (−13.4 – −0.2)</td>
<td>0.77</td>
</tr>
<tr>
<td>RV LEDSR</td>
<td>−3.7 (−10.6 – 5.2)</td>
<td>0.94</td>
<td>5.1 (−6.2 – 15.5)</td>
<td>0.87</td>
</tr>
<tr>
<td>LV LS</td>
<td>0.9 (−4.2 – 4.6)</td>
<td>0.9</td>
<td>2.9 (−2.5 – 12.3)</td>
<td>0.86</td>
</tr>
<tr>
<td>LV LSR</td>
<td>−1.3 (−14.6 – 16)</td>
<td>0.84</td>
<td>2.4 (−9.1 – 16)</td>
<td>0.81</td>
</tr>
<tr>
<td>LV LEDSR</td>
<td>3.0 (−8.2 – 15)</td>
<td>0.82</td>
<td>7.7 (−1.6 – 16)</td>
<td>0.84</td>
</tr>
</tbody>
</table>

Values reported as median (interquartile range) or correlation r-values. All p-values were < 0.01. ICC = intraclass correlation coefficient, LEDSR = longitudinal early diastolic strain rate, LS = longitudinal strain, LSR = longitudinal strain rate, LV = left ventricular, RV = right ventricular.